

1 Multi Modal Medical Image Registration: A New Data Driven 2 Approach

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7 **Abstract**

8 Image registration is a challenging task in building computer-based diagnostic systems. One
9 type of image modality will not be able to provide all information needed for better
10 diagnostic. Hence data from multiple sources/image modalities should be combined. In this
11 work canonical correlation analysis (CCA) based image registration approach has been
12 proposed. CCA provides the framework to integrate information from multiple sources. In
13 this work, the information contained in both images is used for image registration task.
14 T1-weighted, T2- weighted and FLAIR MRI images has Multimodal registration done on it.
15 The algorithm provided better results when compared with mutual information based image
16 registration approach. The work has been carried out using the 3D rigid registration of CT
17 and MRI images. The work is carried out using the public datasets, and later performance is
18 evaluated with the work carried out by Research scholars previously. Our algorithm performs
19 better with mutual information based image registration. Medical image registration of
20 multimodality images like MRI, MRI-CT, and MRI-CT-PET. In this paper for MRI-CT
21 Medical Image Registration CT image is used as a fixed image and MRI image as moving
22 image and later compared results with some benchmark algorithm presented in literature such
23 as correlation coefficient, correlation ratio, and mutual information and normalized mutual
24 information methods.

25

26 **Index terms**— image registration, CCA, CT, MRI, T1, T2, FLAIR, FD, MIR, Rigid registration, MI, NMI,
27 SSD, SAD.

28 **1 Introduction**

29 The medical image registration process is used to estimate the deformation between the images while considering
30 the domain specific Information into consideration. A closer look at the problem statement intuitively reveals
31 two methods of solving it. The first method operates directly on two different images have intensity values called
32 intensity based registration [1], continuously transforming the entire image to align it with the other. When
33 desirable alignment is obtained for the respective transformation, the optical representation is considered to
34 be registered. These methods are called area based methods [2,3]. The second method relies on a few salient
35 points which are most prominent in both the images. The goal here is to estimate the deformation based on the
36 corresponding pairs of points/regions across the images.

37 These are known as feature-based medical picture based on brain methods, have gained popularity over the
38 area based methods These methods [4] are more robust to illumination changes, a partial overlap between the
39 images, occlusion, alterations in background, and viewpoint. Area-based methods are still preferred over feature
40 based techniques, despite these advantages in the medical domain due to two main factors: 1) Its ability to handle
41 local deformations, especially with the case of human organs. 2) Its capability of Dealing with information from
42 different imaging sources.

2 Fig. 1: Image Registration Process a) Transformation

44 Transformation step is to determine the position of corresponding points in reference and sensed images, Medical
 45 Image Registration (MIR) is considered as a combination of translation, rotation, and scaling parameters. Image
 46 registration methods employ transformations such as rigid, affine and elastic (nonrigid transformations [5]. The
 47 rigid transformation considers t_x and t_y translations along the x-axis and yaxis, and a rotational angle θ for
 48 the registration process [6]. It assumes that the subject in the image maintains its shape and size [7]. Affine
 49 transformations offer a high degree of flexibility in accommodating linear distortions by allowing and shearing
 50 in addition to translation and rotation [8]. The non-rigid transformation provides more degree of freedom as
 51 compared to rigid and affine transformation.

52 3 b) Optimization

53 Optimization problem is formulated by a number of parameters used for transformation [9] to get the maximum
 54 value of similarity, for a given registration process. The choice of the transformation is dependent on the type of
 55 application and its geometrical complexity (i.e., degrees of freedom). Although an exhaustive search guarantees
 56 an optimal solution, its computational expense is proportional to the size of the search space as well as the
 57 number of parameters used for transformation and, hence, becomes infeasible as they increase [10]. Therefore,
 58 these forms the motivation to explore refined search strategies or optimization methods which can help to find
 59 the maximum value for a given similarity measure.

Optimization method should be reliable and be capable of finding the best possible transformation quickly [11]. Many optimization methods have been introduced and adopted for the registration process, by the transformation parameters, similarity measure, time restrictions and required accuracy of registration.

63 4 c) Similarity Measure

64 Similarity measure gives the ability to determine the level of global correspondence between two images. During
65 the registration process, the parameters of a given transformation model are changed, based on the optimization
66 technique until the similarity measure reaches a maximum value of alignment [12]. Hence the choice of similarity
67 measure along with optimization method plays a crucial role to a successful outcome of a registration process.

68 5 II. IMAGE REGISTRATION ALGORITHM a) Medical Im- 69 age Registration

70 In Non-rigid registration consists of Non-rigid transformations can be broadly classified by physical models or
 71 basis function expansion. While linear elasticity (Moshfeghi,1991), viscous fluid flow [13] and optical flow [14]
 72 are examples of physical model-based transformations, radial basis functions [15], multi quadrics [16], thin-plate
 73 splines [17], B-spline [18], wavelets [19] and piecewise affine transforms [20] are some of basis function expansion
 74 transformations, involves finding the optimal geometric transformation that maximizes the correspondences across
 75 the images. Medical Image Registration consists of components such as Transformation Model, Similarity Metric
 76 and Optimization Techniques as shown in Fig 1 ?? An image registration algorithm defines an objective function
 77 based on the similarity measure and tries to maximize this objective function. In the proposed method, a new
 78 registration method has been explained using canonical correlation analysis (CCA).

79 6 b) Canonical Correlation Analysis (CCA)

80 Canonical Correlation Analysis (CCA) can be seen as the problem of finding the basis vectors for two set of
 81 variables such that correlation between projections of the variables on these basis vectors is mutually maximized.
 82 CCA seeks a pair of linear or nonlinear transforms one for each step of variables, such that when one set of
 83 variables, is transformed, the corresponding coordinates are maximally correlated. CCA used in image retrieval,
 84 image fusion [21] and object recognition problems [22] in computer vision.

85 CCA finds the relationship between two multidimensional datasets [21]. The basic formulation of CCA is as
86 follows:

87 For a given two multi-dimensional data sets of basis vectors or projection vectors wx, wy respectively, for two
 88 data sets that maximize the correlation between the random variables $x=w x^T (xi-x)$ and $y= w y^T (yi-y)$,??
 89 = ??[??,??] ??[?? 2]??[?? 2] = ??[???? ? ?? ????? ? ???? ?] ???? ????? ? ???? ? ? ????[???? ?? ?
 90 ????? ? ? ????? ?]

$$(2.1) ?? = ????? ? ?? ?????????????] ?? ????. ?? ?????????????? ???. ?? ?? ?????????????? (2.2)$$

92 C_{xx} and C_{yy} are the within-class covariance matrix and, C_{xy} is the cross -covariance matrix. Maximum
 93 correlation has been found as follows. $\hat{W} = \text{argmax} (W x T C_{xy} Y T W y) \quad (2.3)$ s.t $W x T C_{xx} W x = 1$ and
 94 $W y T C_{yy} W y = 1$ **(2.4)**

95 The Basic formulation of CCA has the following disadvantage. 1. CCA finds the only linear relationship
96 between two datasets. 2. Difficult to extend more than two data sets.

97 These problems can be addressed using the following ways. 1. A non-linear relationship between the data sets
 98 can be addressed using kernel extension of CCA [23].

99 Kernel CCA defines the non-linear mapping of two datasets $\mathbf{?} : \mathbf{x} \rightarrow \mathbf{?}(\mathbf{x})$ and $\mathbf{?} : \mathbf{y} \rightarrow \mathbf{?}(\mathbf{y})$ and performs the
100 traditional CCA on transformed datasets. 2. Neural network based CCA extracts the non-linear relationship
101 between datasets. 3. Locality preserving method based CCA also extracts a non-linear relationship between
102 datasets.

103 **7 III. Algorithm for Image Registration**

104 Image Registration methods are trying to find the relationship between two images in intensity domain or feature
105 domain. Regarding similarity measures this relationship is defined. Similarity measures can be classified in two
106 categories (i) in all; similarity measure quantifies the spatial alignment between two images. Various intensity-
107 based similarity measures such as sum of squared difference (SSD) [24], sum of absolute difference (SAD) [25],
108 correlation coefficient (CC) [26], NCC [27] and ratio image uniformity (RIU) [28] have been proposed for mono
109 modal registration process. These measures do not perform well in all cases. While SSD [25] is highly sensitive
110 to Gaussian noise, SAD is less responsive to outliers on the subject boundaries. CC, NCC and, RIU perform well
111 in these conditions, but are highly sensitive to non-uniform illumination in the images and (ii) The Non-linear
112 similarity measures such as mutual information or divergence measures, etc. Multimodal image registration, the
113 images are captured through different sensors (CT or MRI) or different parameters (T1, T2 or FLAIR) so that
114 the intensity relationships between images are highly non-linear.

115 In this work, based on the structural representation of images an algorithm has been proposed. The dense
116 set of descriptors which perform the intensity based registration replace the input images. The advantage of this
117 method is that after new representation, one can use any simple similarity measure such as L2 norm or SSD [25]
118 for multimodal image registration.

119 **8 Given two images find projection directions using**

120 Kernel CCA (Gaussian kernel used for projection). 2. Project original images or features in lower dimension
121 space using projection direction. 3. Use L2 norm as a similarity measure.

122 In this algorithm Gradient descent uses $\mathbf{?}$ optimization function.

123 **9 IV. Methodology**

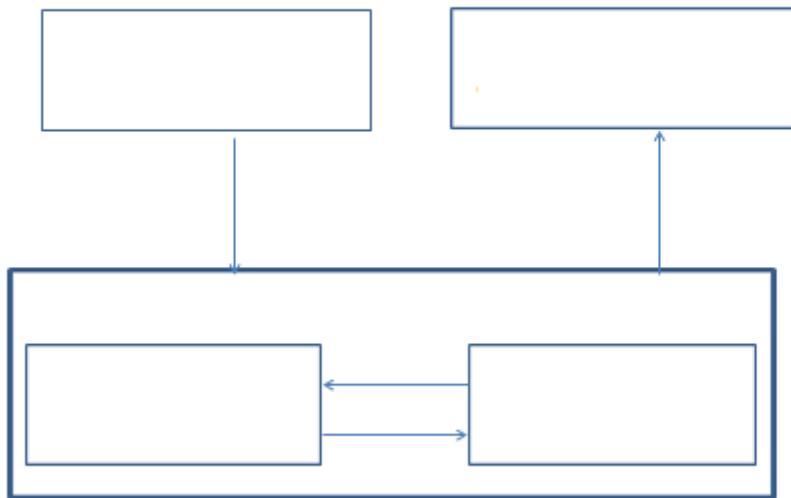
124 Using two sets of experiments the work has been carried out and is detailed below 1. First set of demonstrations
125 on T1 and T2 MR Images for 3D rigid registration (RIRE dataset). Experiments are carried out with the
126 specifications: 15mm translation and 10-degree rotation as a deviation from correct position with ten times with
127 different affine parameter settings. Mutual information based method for rigid registration has been used to be
128 compared against the experimental results. We show the absolute error for translation (in mm), rotation (in
129 degree) and root mean square error (RMS) in Tab. 1. Consider 1 mm equal to 1 degree for the absolute error
130 computation. CCA has been performed on for more than two modalities (T1, T2, and PD) also. Tab. 2 Shows
131 results for Brain web dataset. Comparison purpose uses the MI based on pairwise registration framework. CCA
132 based method performs better regarding accuracy (Tab1) (in translation and rotation) compared to MI-based
133 method. CCA based method improves overall accuracy to 6.7% in pairwise registration and 13 % in Groupwise
134 registration compared MI-based method. The Degree of freedom: 9 0 The work has been carried out using two
135 sets of experiments and are detailed below. ??able 1: For the error calculation, five manual points were marked
136 on the MRI image. In the second set of images also the experiments in a similar environment and the same
137 method are used for error calculation. Results have been shown in following Tab.4.

138 **10 V. Results**

139 **11 a) Figures and Tables**

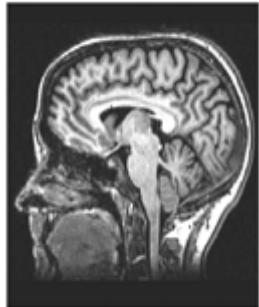
140 **12 Conclusion**

141 In this work new algorithm, CCA has been proposed for image registration. In multimodal framework, due
142 to different acquisition parameters, the relation between datasets not follows the linear relationship. In this
143 algorithm, the kernel version of canonical correlation analysis was used because the basic formulation of CCA
144 gives the only linear relationship between datasets. The results are shown in Table ??, Table ??I Two sets of
145 experiments have been performed on the RIRE datasets (T1, T2, and PD images). (i) Pair wise registration
146 and (ii) Group-wise registration. From table I, Table ??I, it is evident that group-wise registration performs well
147 compared to pairwise registration because group-wise registration consists of extra information (due to other
148 modalities) which helps registration. The advantage of using CCA based method is one can easily extend this
149 framework for more than two modalities. ¹



2

Figure 1: Fig. 2 :



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Figure 2: Fig. 5 Fig. 3 :

2

Method	Translation x(mm)	Translation y(mm)	Rotation (Degrees)
MI-based	3.1	2.0	4.2
CCA	2.9	1.8	4.0

Figure 3: Table 2 :

3

Moving image	Static image
Registered Image_MI	Registered image_CCA

Figure 4: Table 3 :

4

[Note: provide bone structure information and, MRI dispenses soft tissue information of brain. For accurate tumor diagnostic one needs CT and MRI information. In this work 3D, rigid registrations of CT and MRI images were performed. In this work CT image used as the fixed image and MRI image as moving image. On comparing results with some benchmark, algorithm presents in literature such as mutual information; normalize mutual information and correlation-based approaches.]

Figure 5: Table 4 :

5

Figure 6: Table 5 :

Figure 7:

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12 CONCLUSION

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